



ISNVD
International Society for
Neurovascular Disease

The X ISNVD Annual Meeting

Measuring respiratory and cardiac influences on blood and cerebrospinal fluid flow with real-time MRI

Maria Marcella Laganà^{1,*}, Alice Pirastru^{1,2}, Sonia Di Tella^{1,3}, Francesca Ferrari², Laura Pelizzari¹, Marta Cazzoli¹, Noam Alperin⁴, Ning Jin⁵, Domenico Zacà⁶, Giuseppe Baselli⁷, Francesca Baglio¹

1. IRCCS Fondazione Don Carlo Gnocchi ONLUS, Milan, Italy; 2. Department of Electronics, Information, and Bioengineering, Politecnico di Milano, Milano, Italy; 3. Università Cattolica del Sacro Cuore, Department of Psychology, 20123 Milan, Italy; 4. University of Miami, Miami, USA; 5. MR R&D Collaborations, Siemens Medical Solutions USA, Inc., Cleveland, Ohio, USA; 6. Siemens Healthcare, Milano, Italy



Maria Marcella Laganà – marcella.lagana@gmail.com

1



ISNVD
International Society for
Neurovascular Disease

The X ISNVD Annual Meeting

Declaration of Financial Interests or Relationships

- Maria Marcella Laganà: I have no financial interests or relationships to disclose with regard to the subject matter of this presentation.
- Ning Jin works for MR R&D Collaborations, Siemens Medical Solutions USA, Inc., Cleveland, Ohio, USA
- Domenico Zacà works for Siemens Healthcare, Milano, Italy

2

Introduction

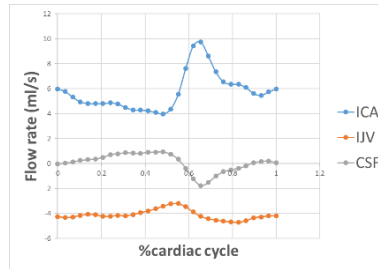
- Venous and CSF flow alterations have been described in various neurological conditions¹
- Cerebrospinal fluid (CSF) flow: crucial role in the brain waste clearance (glymphatic system)²



Conventional flow quantification: cine cardiac-gated Phase Contrast (PC) MRI

BUT:

- 1) heart rate variability
- 2) respiration modulates venous return and CSF flow³ [thoracic pump]



1. Zivadinov et al., BMC Med 2013; Attier-Zmudka et al., Front Aging Neurosci 2019; Jakimovski et al., Fluids and Barriers of the CNS 2020
 2. Iliff et al., Sci Transl Med 2012
 3. Zamboni et al., J Appl Physiol 2012;
 Laganà et al., Ultrasound in Medicine and Biology, 2017

3

Introduction

- Venous and CSF flow alterations have been described in various neurological conditions¹
- Cerebrospinal fluid (CSF) flow: crucial role in the brain waste clearance (glymphatic system)²



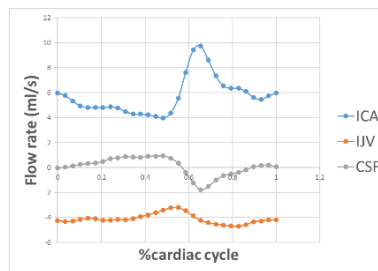
Conventional flow quantification: cine cardiac-gated Phase Contrast (PC) MRI

BUT:

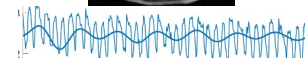
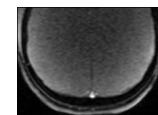
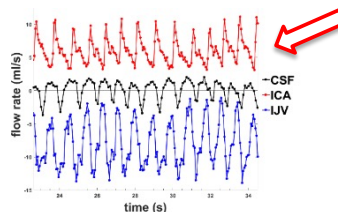
- 1) heart rate variability
- 2) respiration modulates venous return and CSF flow³ [thoracic pump]



Real-time (RT) PC MRI⁴ for assessing flow rate respiratory modulations



1. Zivadinov et al., BMC Med 2013; Attier-Zmudka et al., Front Aging Neurosci 2019; Jakimovski et al., Fluids and Barriers of the CNS 2020
 2. Iliff et al., Sci Transl Med 2012
 3. Zamboni et al., J Appl Physiol 2012;
 Laganà et al., Ultrasound in Medicine and Biology, 2017
 4. Ohno et al., Diagnostics 2020; Yildiz et al., JMRI 2017



4

Aims

Study 1 – Beat-by-beat variability

Aim 1 - Assess the blood and CSF beat-by-beat variability

Aim 2 - Compare the flow rate obtained using the RT-PC and the clinical cardiac-gated cine PC sequence



Real-Time Phase-Contrast MRI to Monitor Cervical Blood and Cerebrospinal Fluid Flow Beat-by-Beat Variability.
Baselli et al., *Biosensors* 2022, 12(6), 417

Study 2 – Blood and CSF flow drivers

Aim 1 - Testing the presence of the cardiac and respiratory drivers

Aim 2 - Assessing how different breathing modes affect the:

(A) mean flow rate

(B) respiratory and cardiac modulations to the flow rate



Blood and cerebrospinal fluid flow oscillations measured with real-time phase-contrast MRI: breathing mode matters. Laganà et al., *FBCNS. Preprint at Research Square* [<https://doi.org/10.21203/rs.3.rs-1722506/v1>]

Study 3 – Intra and extracranial venous flow

Aim - Assessing cardiac and respiratory modulations on intracranial (sup sagittal sinus) and neck venous flow



Cardiac and Respiratory influences on intracranial and neck venous flow measured with Real-Time Phase-Contrast MRI. Laganà et al., *Biosensors* 2022.

5

Materials and Methods

Subjects

Healthy volunteers
N=30 (21 females)
age: 26[19-57] years



MRI Scanner

3T Siemens Prisma
64-channel head-neck coil



MRI acquisition protocol

- Prototype RT-PC (acquired for 60 s)
- Respiration:
 - normal free breathing (F)
 - paced normal (PN)
 - paced deep breathing (PD)



Measuring	RT-PC Positioning	Venc (cm/s)	Temporal resolution (ms)	#time points
A) blood	Perpendicular to neck vessels	70	58.5	1021
B) CSF	Perpendicular to spinal cord	6	94	637
C) SSS	Perpendicular to the sup sag sinus	40	58.5	1021

6

Materials and Methods

Subjects

Healthy volunteers
N=30 (21 females)
age: 26[19-57] years



MRI Scanner

3T Siemens Prisma
64-channel head-neck coil



MRI acquisition protocol

- Prototype RT-PC (acquired for 60 s)
- Respiration:
 - normal free breathing (F)
 - paced normal (PN)
 - paced deep breathing (PD)
- Physiologic signals:
 - respiration with an abdominal band
 - pulse with a pulse oximeter

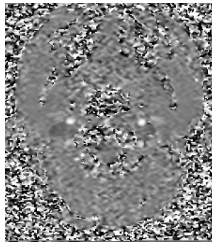


Measuring	RT-PC Positioning	Venc (cm/s)	Temporal resolution (ms)	#time points
A) blood	Perpendicular to neck vessels	70	58.5	1021
B) CSF	Perpendicular to spinal cord	6	94	637
C) SSS	Perpendicular to the sup sag sinus	40	58.5	1021

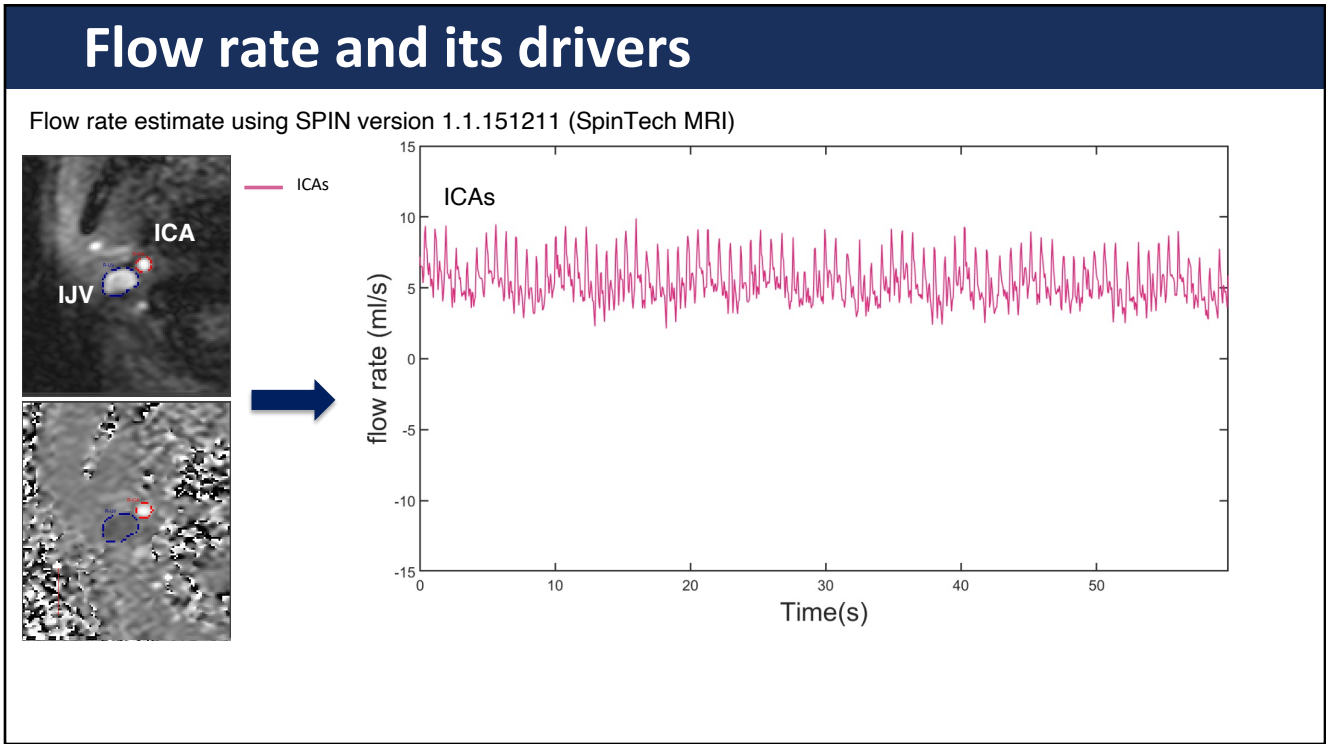
7

Flow rate and its drivers

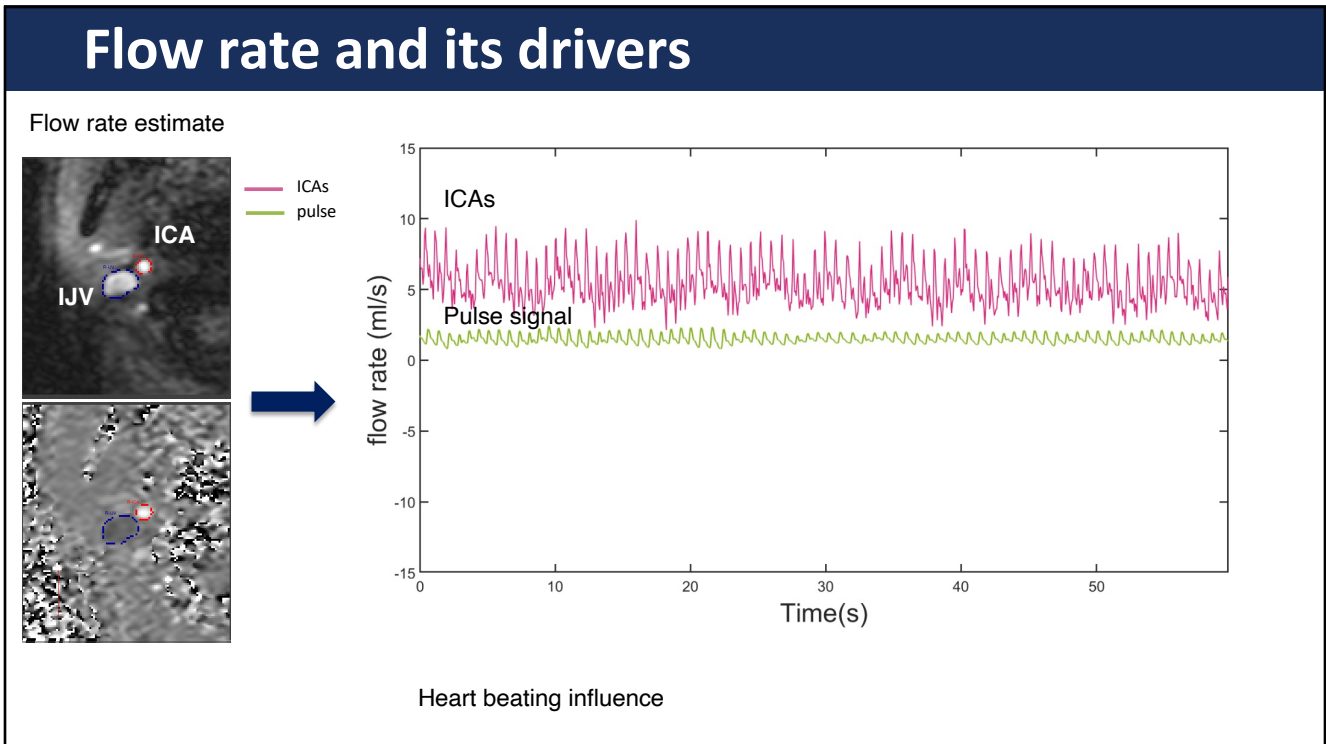
Magnitude and Phase images: neck blood



8



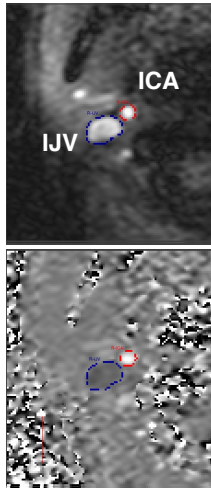
9



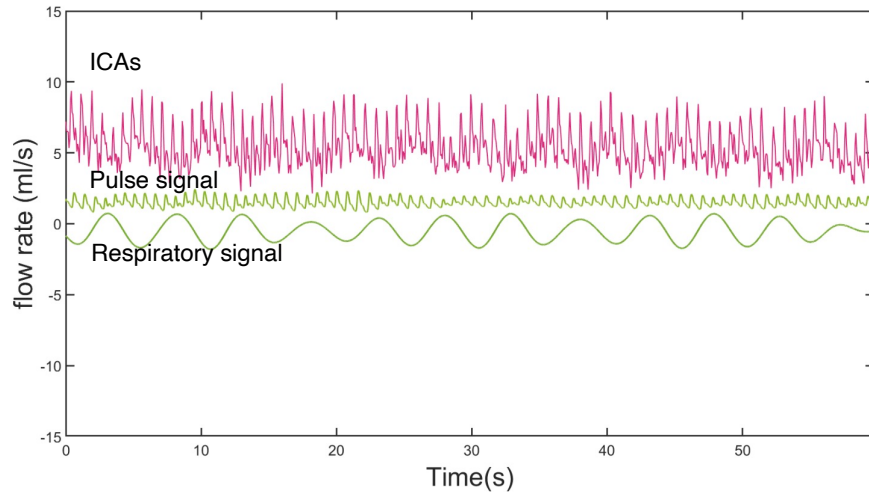
10

Flow rate and its drivers

Flow rate estimate



— ICAs
— pulse
— resp

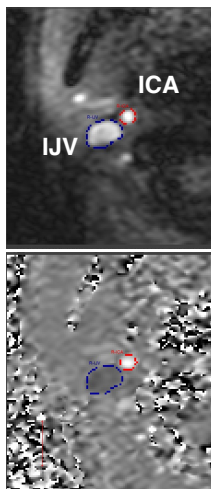


Respiratory pump influence

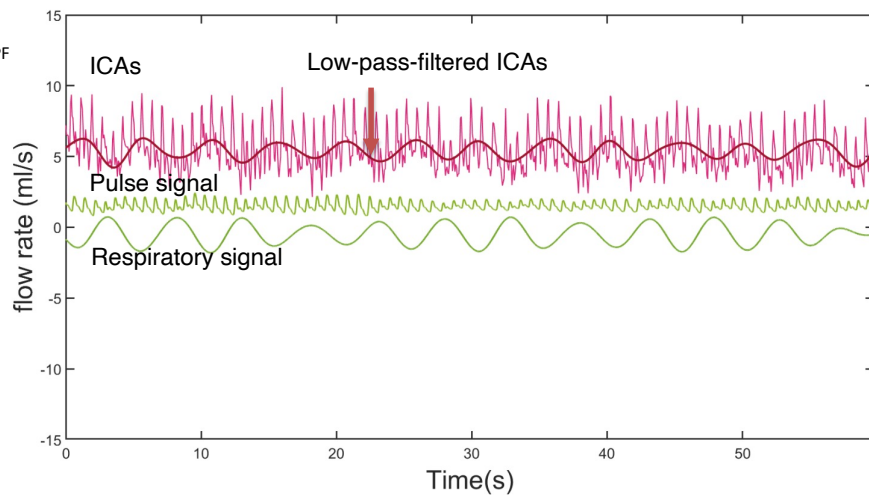
11

Flow rate and its drivers

Flow rate estimate



— ICAs+LPF
— pulse
— resp

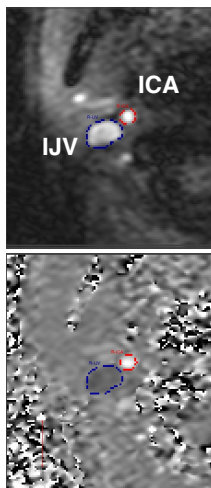


Respiratory pump influence

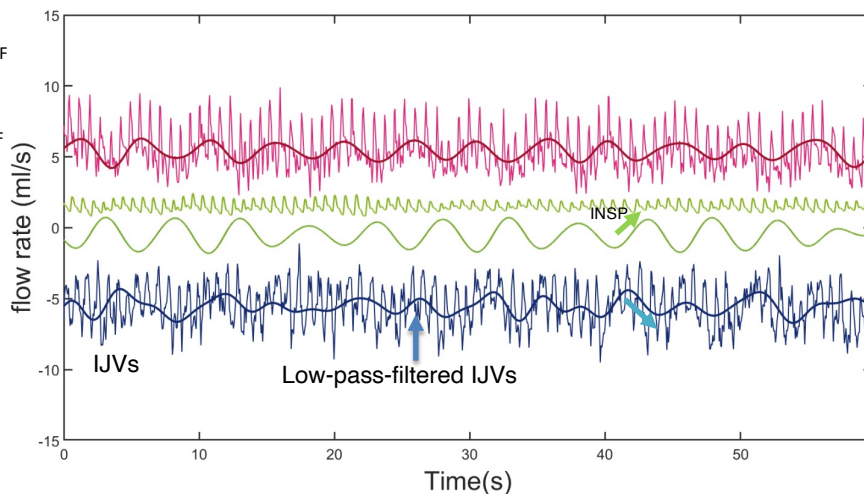
12

Flow rate and its drivers

Flow rate estimate



- ICAs+LPF
- pulse
- resp
- IJVs+LPF

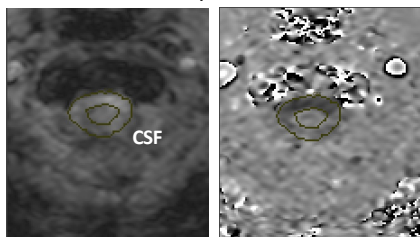


Cardiac and respiratory pump influence

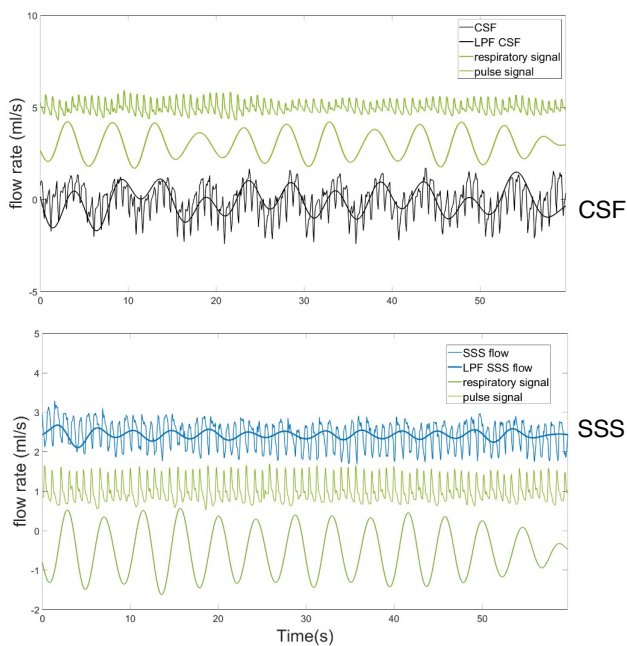
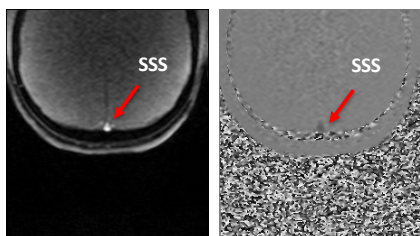
13

Flow rate and its drivers

Cervical cerebrospinal fluid flow



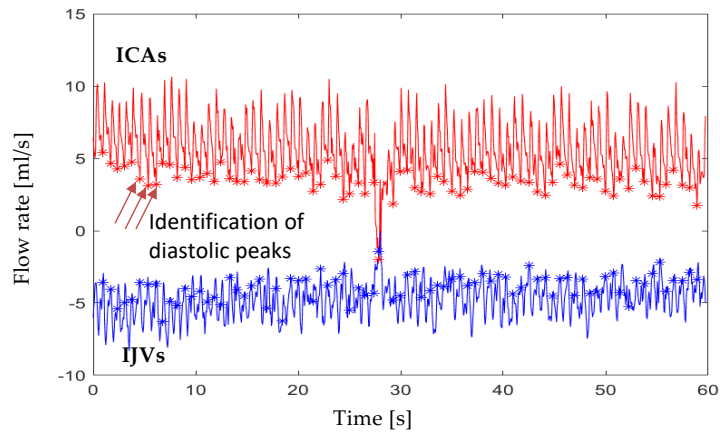
Superior sagittal sinus



14

Study 1 – Beat-by-beat variability

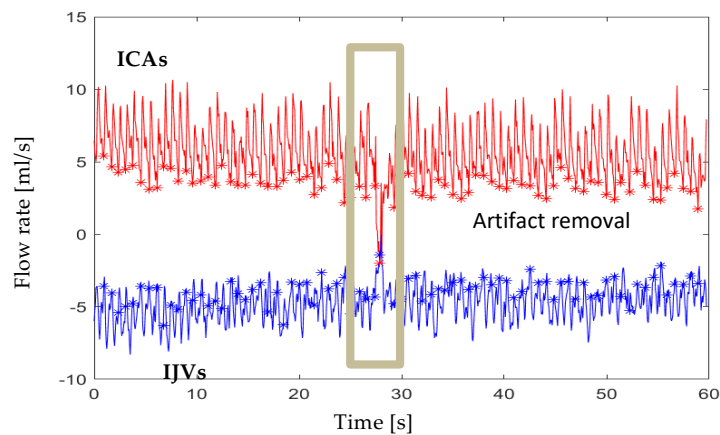
- Identification of diastolic peaks



15

Study 1 – Beat-by-beat variability

- Identification of diastolic peaks
- Artifact removal (removal of artifacted signal windows)



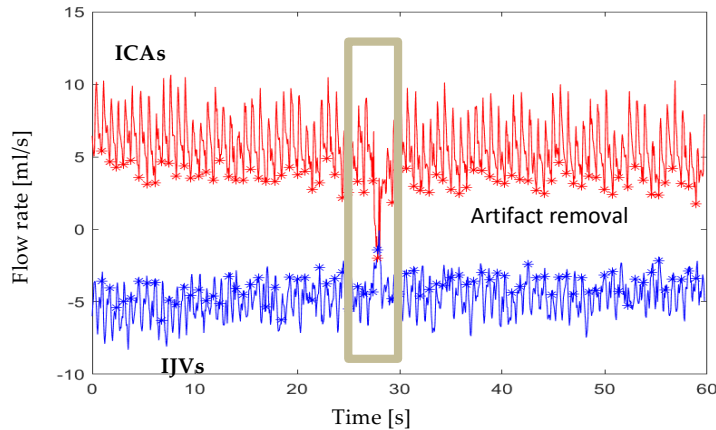
Baselli et al., Biosensors 2022, 12(6), 417

16

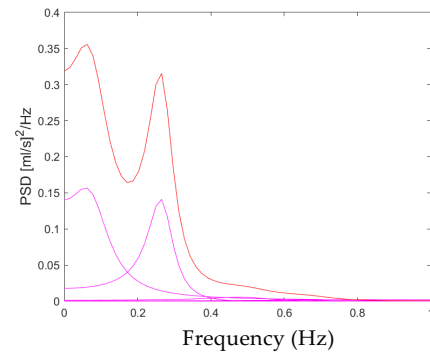
Study 1 – Beat-by-beat variability

- Identification of diastolic peaks
- Artifact removal (removal of artifacted signal windows)
- Study of the systolic/diastolic peaks, heart rate, beat-by-beat variability (autoregressive models, as for ECG signal*)

*Baselli et al., IEEE Trans Biomed Eng, 1988

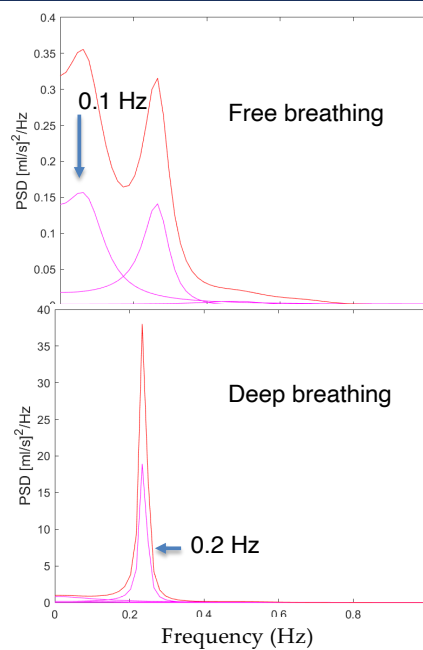


Baselli et al., Biosensors 2022, 12(6), 417



17

Study 1 – Beat-by-beat variability



Autoregressive power spectral density

- Modulations at the respiratory frequency and at a lower frequency (around 0.1 Hz): **Mayer waves**, seen both in the ECG and in continuous blood pressure curves
- Oscillations of the sympathetic vasomotor tone of arterial blood vessels.
 - It has been suggested that Mayer waves trigger the liberation of endothelium-derived nitric oxide (NO) by cyclic changes of vascular shear stress¹
 - "the frequency shift of Mayer waves to lower frequencies is associated with an increased risk of developing established hypertension"²

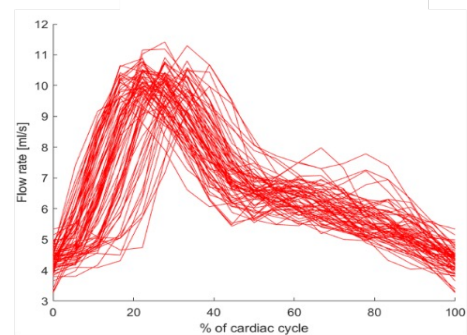
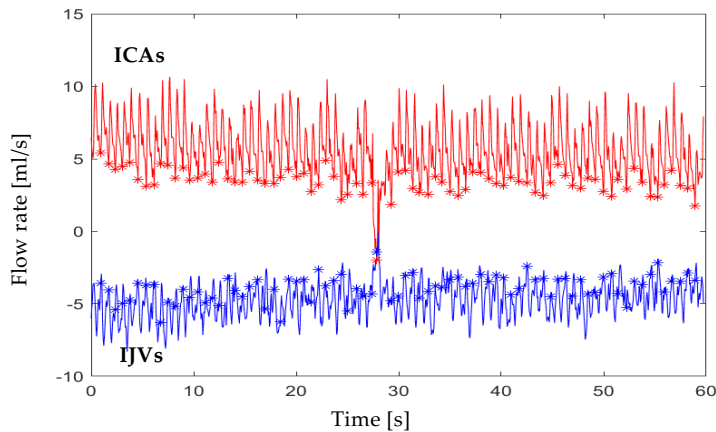
¹Julien. Cardiovasc Research 2006

²Takalo et al., American Journal of Hypertension 1999

18

Study 1 – Beat-by-beat variability

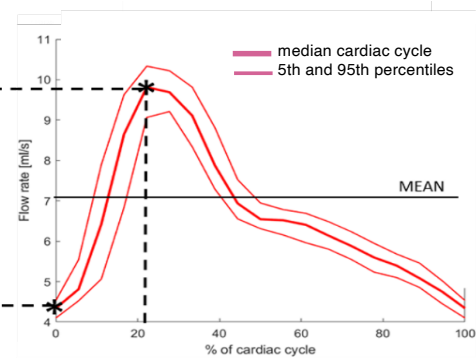
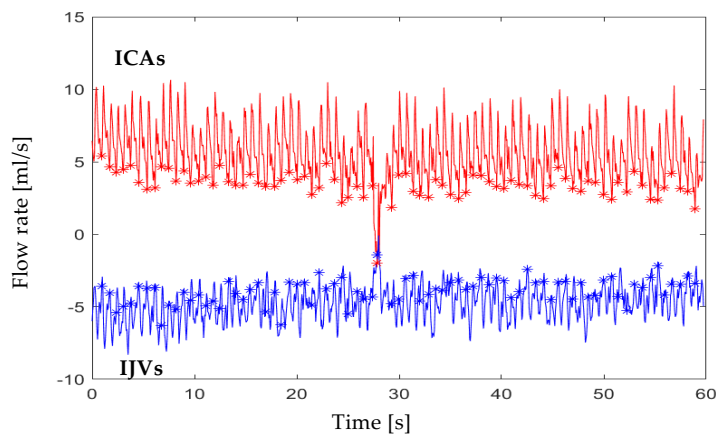
- Identification of diastolic peaks
- Artifact removal (removal of artifacted signal windows)
- Alignment of cardiac cycles, beginning from diastolic peak



19

Study 1 – Beat-by-beat variability

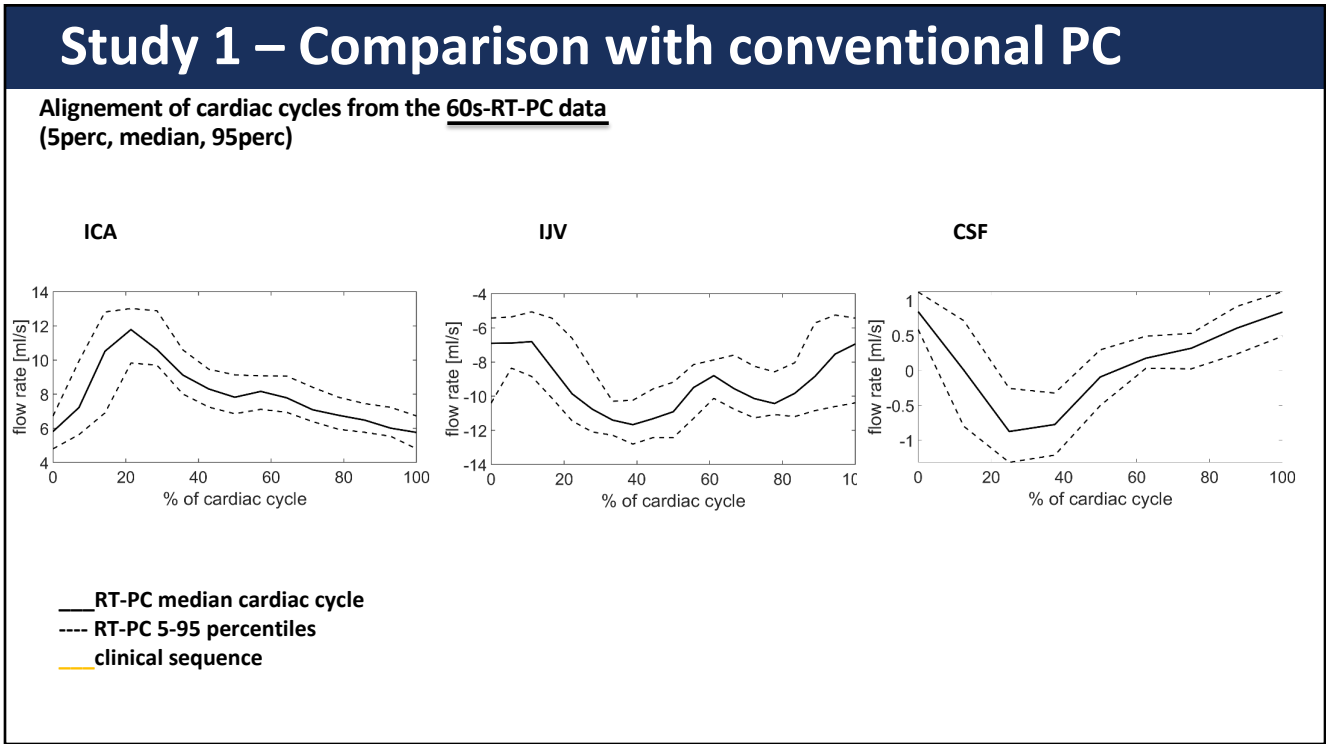
- Identification of diastolic peaks
- Artifact removal (removal of artifacted signal windows)
- Alignment of cardiac cycles, beginning from diastolic peak → median curve for each subject



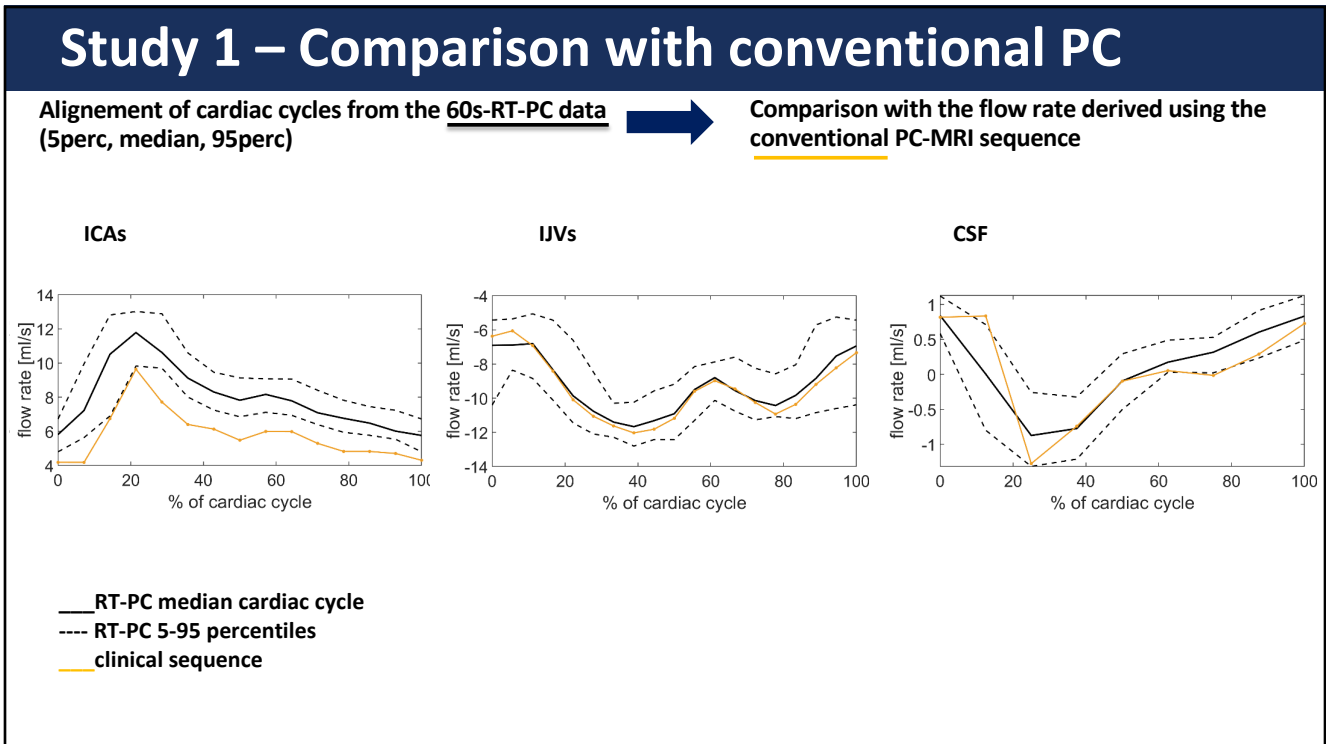
Median curve, 5th and 95th percentiles

Baselli et al., Biosensors 2022, 12(6), 417

20



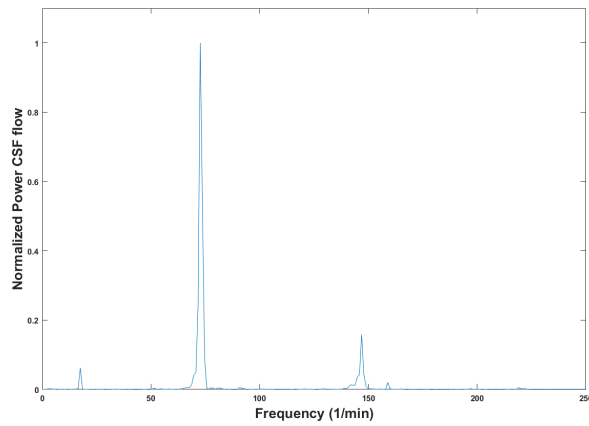
21



22

Study 2 – Blood and CSF flow drivers

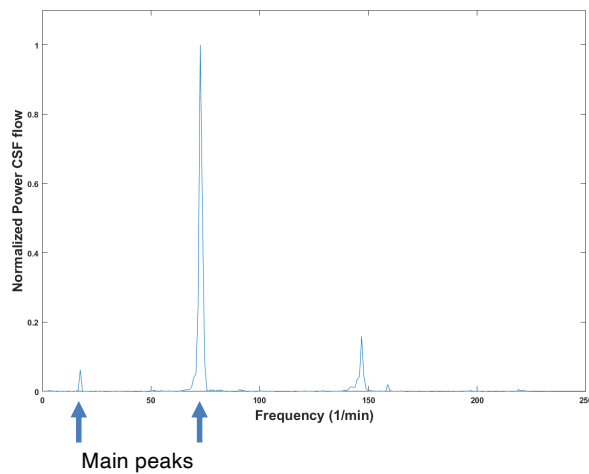
- Power Spectral Density of the flow rate



23

Study 2 – Blood and CSF flow drivers

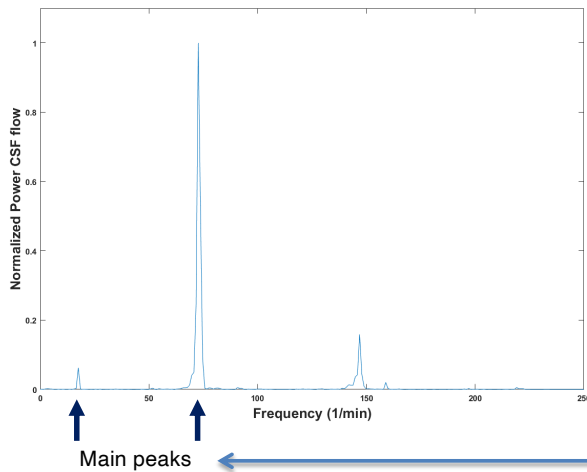
- Power Spectral Density of the flow rate
- Identification of main peaks



24

Study 2 – Blood and CSF flow drivers

- Power Spectral Density of the flow rate
- Identification of main peaks
- Breathing rate and heart rate computed from physiologic signals



Breathing rate (BR) from thoracic band



Heart rate (HR) from pulse oximeter

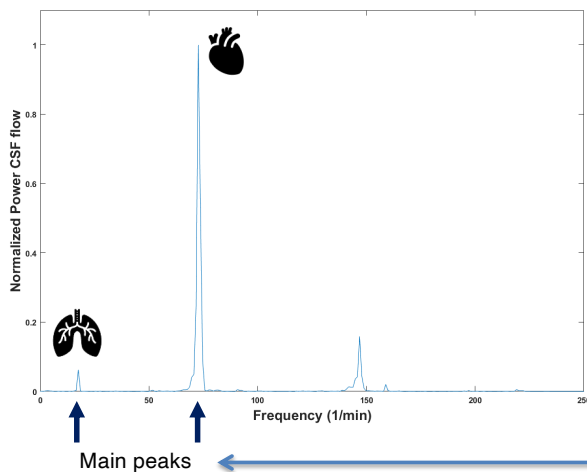


Frequencies comparison

25

Study 2 – Blood and CSF flow drivers

- Power Density Spectrum of the flow rate
- Identification of main peaks
- Breathing rate and heart rate computed from physiologic signals
- Peak frequencies compared to breathing rate and heart rate



Breathing rate (BR) from thoracic band



Heart rate (HR) from pulse oximeter



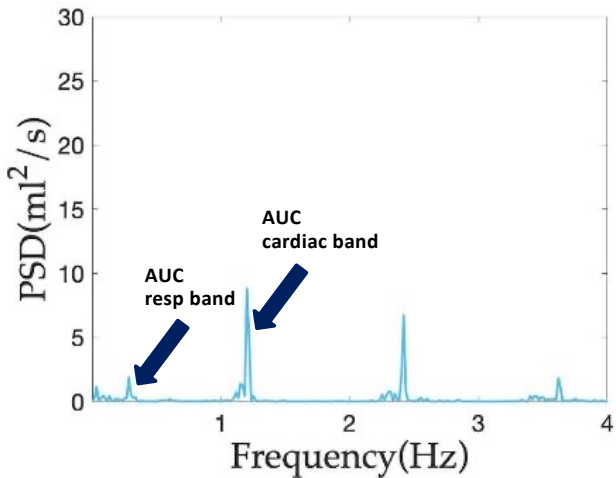
Frequencies comparison:

- First peak: not significantly different compared to the BR
- Second peak: not different compared to the HR

26

Study 2-3 – cardiac and respiratory modulations

- Area under the curve (AUC) of the respiratory and cardiac bands (power in $[ml/s]^2$)
- AUC to the signal variance (NAUC) \rightarrow adimensional index [0-1]



Indices for quantifying the respiratory and cardiac modulations:

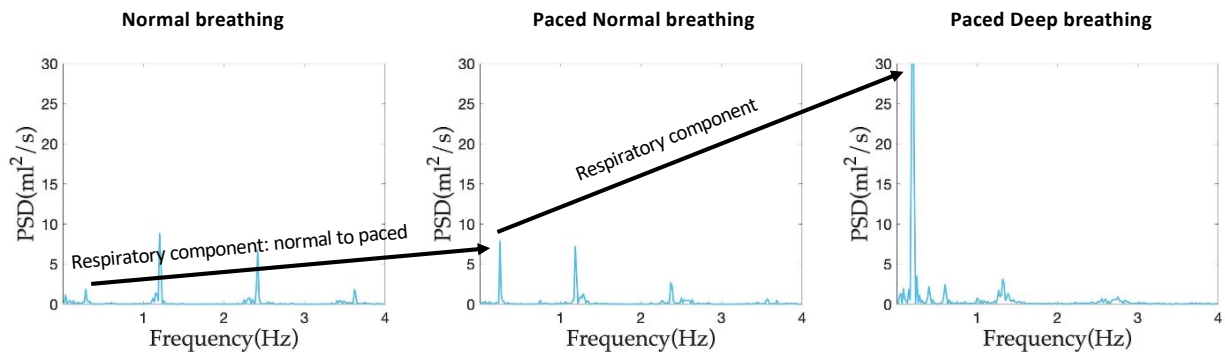
- NAUC_resp
- NAUC_card
- Respiratory/Cardiac = AUC_resp/AUC_card

What happens with different breathing modes?

27

Study 2-3 – cardiac and respiratory modulations

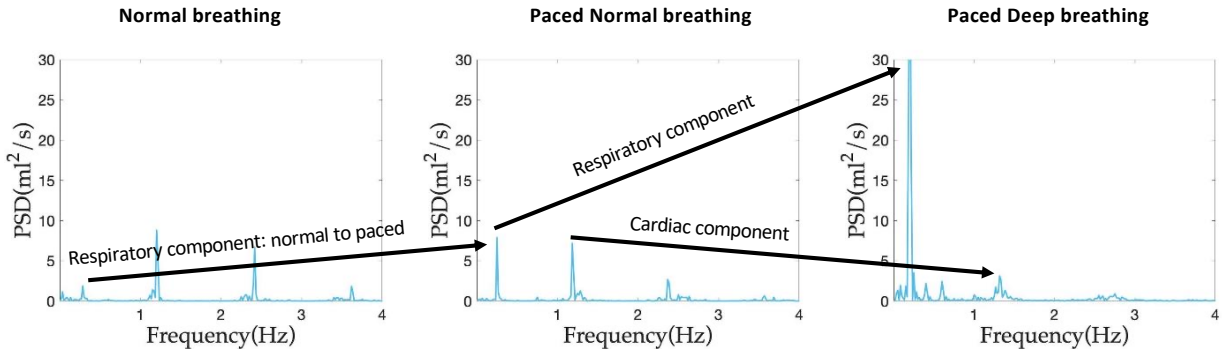
Single subject: IJV flow rate spectrum



28

Study 2-3 – cardiac and respiratory modulations

Single subject: IJV flow rate spectrum



29

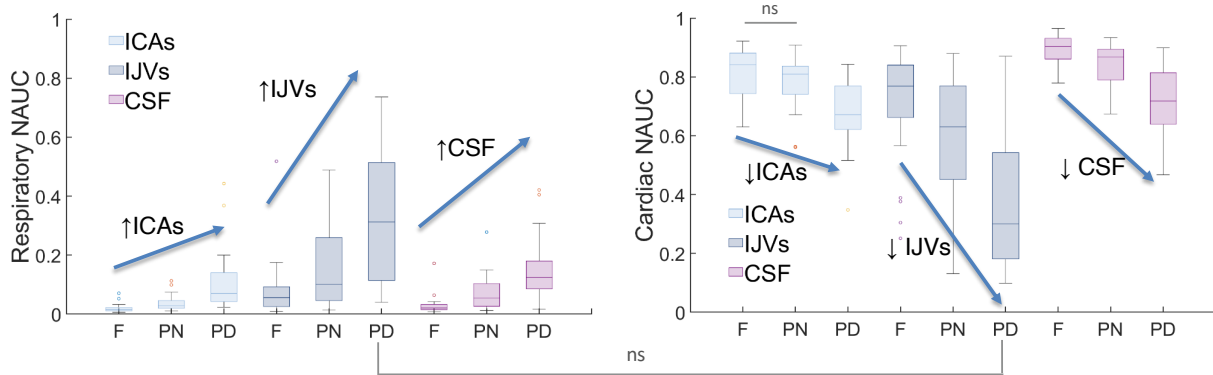
Study 2 – cervical flow rate modulations

Group analysis: respiratory and cardiac components

What happens from free (F) to paced normal (PN) to paced deep (PD) breathing?

- Respiratory component \uparrow ($p < 0.001$)
- Cardiac component \downarrow ($p < 0.001$)
- Cardiac > respiratory component ($p < 0.001$)

With the exception of non-significant comparisons written in the graph

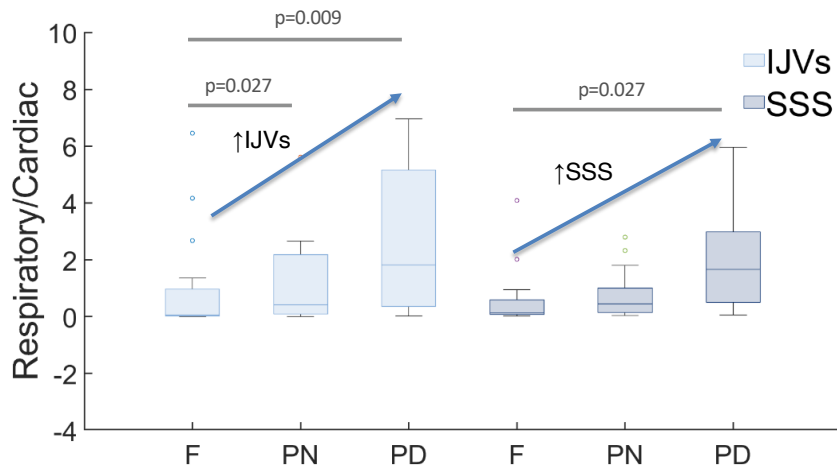


30

Study 3 – intracranial vein flow rate modulations

Group analysis: respiratory and cardiac modulation changes

- Respiratory/cardiac component increment from free (F) to paced normal (PN) to paced deep (PD) breathing

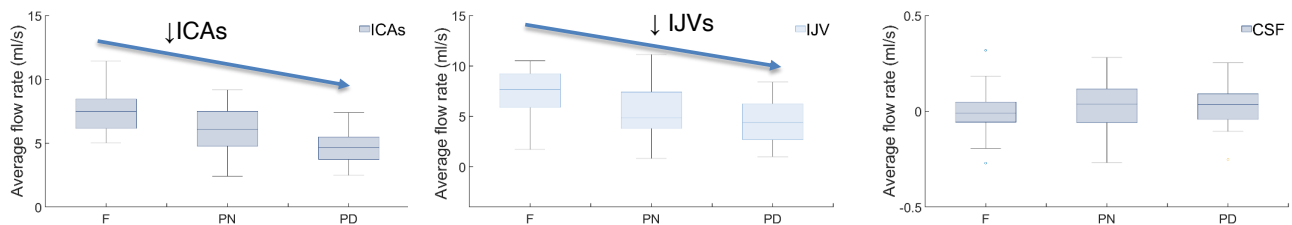


31

Study 2 – average cervical flow rate

Group analysis: flow rate and area changes

- Blood average flow rate decrement ($p < 0.001$ for all the paired comparisons)

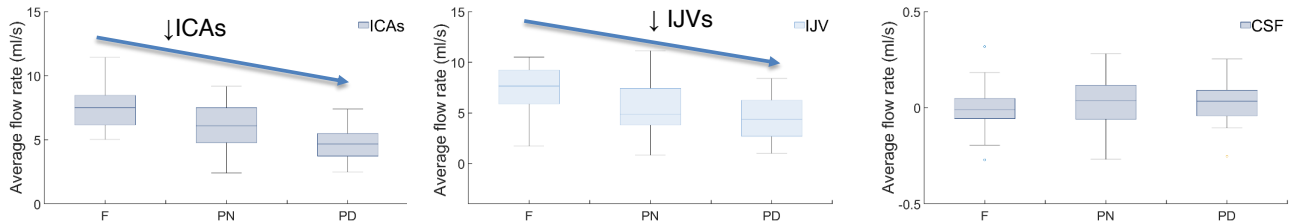


32

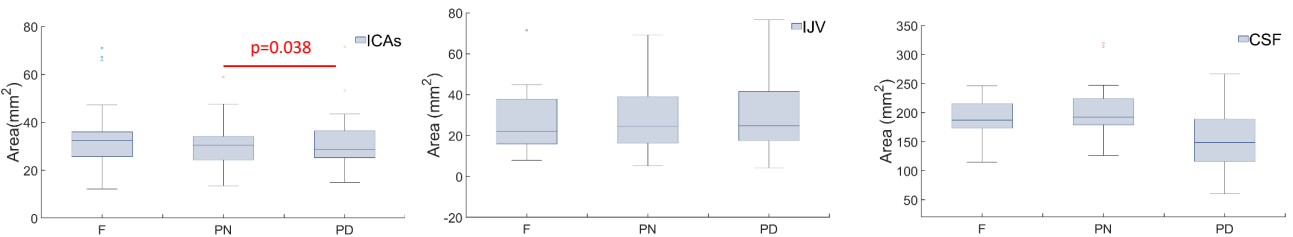
Study 2 – average cervical flow rate

Group analysis: flow rate and area changes

- Blood average flow rate decrement ($p < 0.001$ for all the paired comparisons)



- Cross-sectional area decrement for ICA only (smallest in deep breathing)

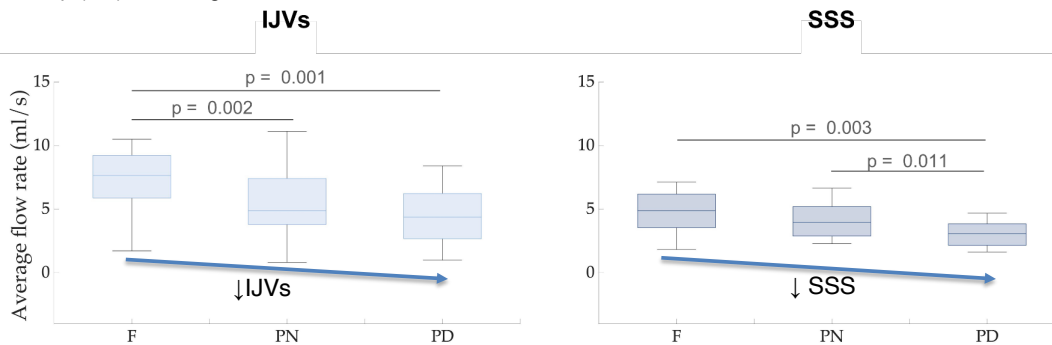


33

Study 3 – intracranial average flow rate

Group analysis: flow rate and cross-sectional area changes

- Blood average flow rate decrement ($p < 0.001$ for all the paired comparisons) from free (F) to paced normal (PN) to paced deep (PD) breathing



- Cross-sectional areas do not change

34

Conclusions



Prototype RT-PC for measuring blood and CSF flow rates with **high temporal resolution** allows to **quantify** not only the cardiac but also the respiratory influence and the low-frequency modulations.



The beat-to-beat changes with HR variability can be studied

35

Conclusions



Prototype RT-PC for measuring blood and CSF flow rates with **high temporal resolution** allows to **quantify** not only the cardiac but also the respiratory influence and the low-frequency modulations.



The beat-to-beat changes with HR variability can be studied



From normal to deep breathing:
mean flow ↓ (vasoreactive response, ↓ CO₂ blood concentration?)



From normal to deep breathing:
respiratory modulation ↑ (greater effect of the thoracic pump) and cardiac modulation ↓ for cervical CSF, arterial and venous flow, but also for the superior sagittal sinus

36

Conclusions



Limitations:

- Only supine position
- Separate acquisitions of blood and CSF flows
- Limited spatial resolution
- Image movement artifacts during deep breathing
- CO2 blood concentration was not measured

37

Conclusions



Limitations:

- Only supine position
- Separate acquisitions of blood and CSF flows
- Limited spatial resolution
- Image movement artifacts during deep breathing
- CO2 blood concentration was not measured



Clinical studies: RT-PC MRI used in pathological cases might allow to investigate how the flows in/out the brain are modulated by breathing patterns.

- Various pathologies might change respiration during sleep → effects on CSF circulation?
- Arterial-venous-CSF flows are linked (Monro-Kellie): might venous alterations change CSF flow?
- Impact of respiration type for drug delivery through CSF

38

Acknowledgments



Francesca Baglio

Marta Cazzoli

Sonia Di Tella

Laura Pelizzari

Alice Pirastru



Noam Alperin



Ning Jin

Domenico Zacà



Giuseppe Baselli

Students: Ferrari, Fasani, Caglioni, Cavallini, Giudetti, Giudici

Maria Marcella Laganà – marcella.lagana@gmail.com

39

backup

40

RT-PC prototype

- Developed for cardiovascular applications
- Echo planar imaging readout module
- Parallel acceleration in the temporal direction (T-PAT).
- Novel reconstruction algorithm, shared velocity encoding (SVE)* to improve temporal resolution →

2-sided velocity encoding: also called symmetric or bipolar encoding. It acquires a positive (k_+) velocity encoded and a negative velocity encoded (k_-) acquisition for each cardiac phase to produce the phase difference image.

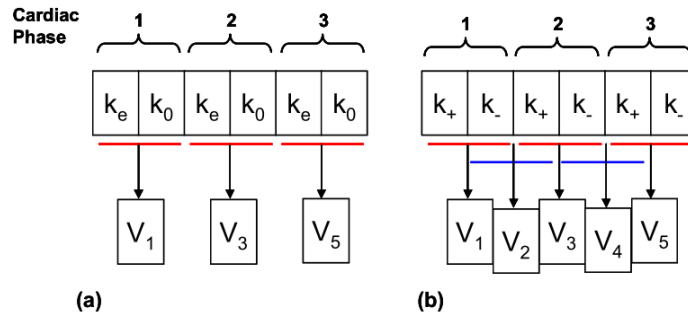


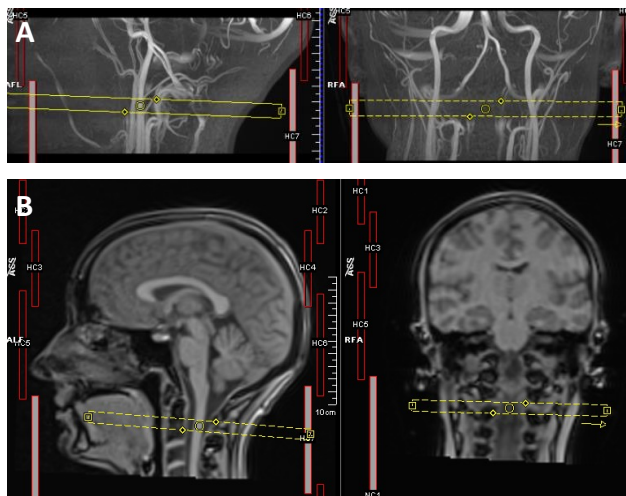
Figure 4. (a) The conventional PC with 1-sided velocity encoding. Velocity information was extracted using the flow encoded (k_e) and flow compensated (k_0) data within the same cardiac phase. (b) SVE with 2-sided velocity encoding. Additional velocity frames (V_2 and V_4) are reconstructed by sharing the flow encoded data across cardiac phases to double the effective frame rate by a factor of 2.

*Lin H et al. Magn Reson Med. 2011

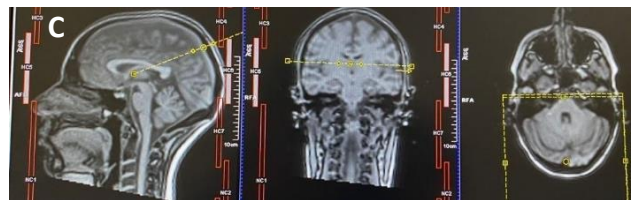
41

Methods: positioning

Extracranial acquisitions

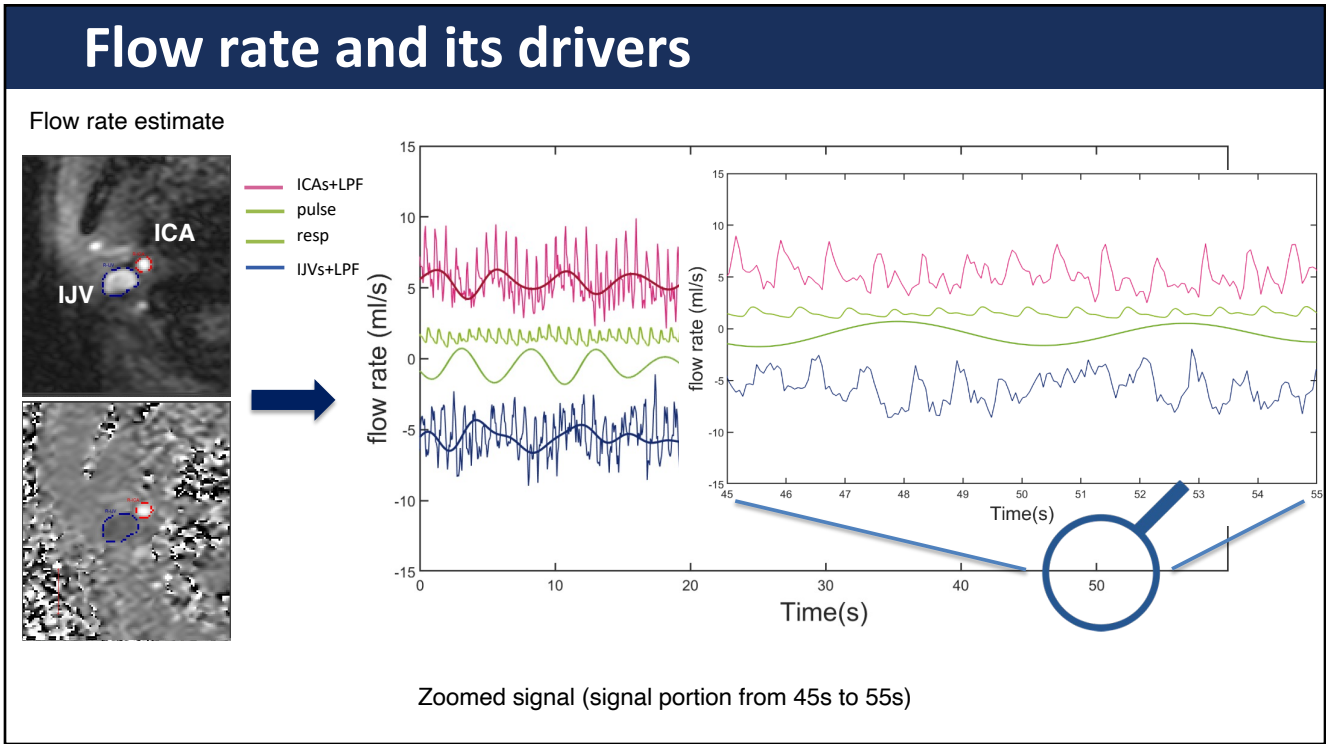


Intracranial acquisition

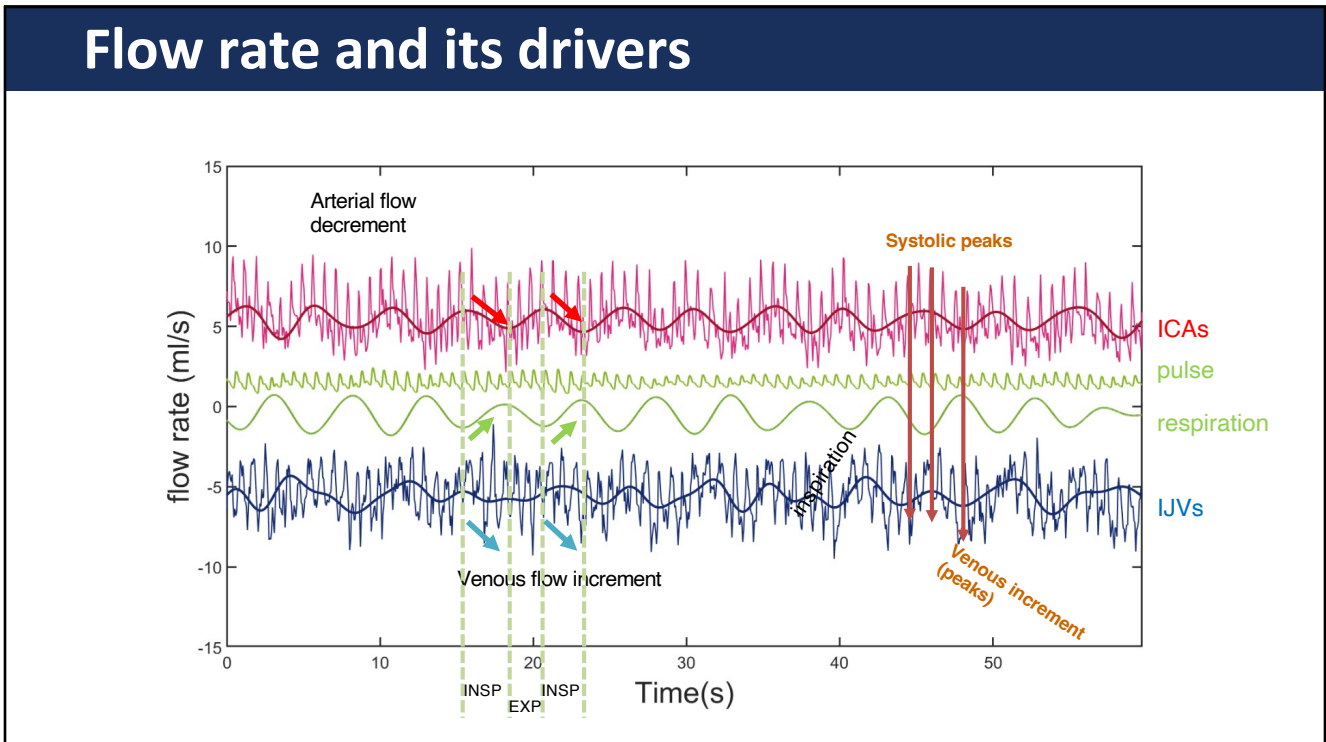


Measuring	RT-PC Positioning	Venc (cm/s)	Temporal resolution (ms)	#time points
A) blood	Perpendicular to neck vessels	70	58.5	1021
B) CSF	Perpendicular to spinal cord	6	94	637
C) SSS	Perpendicular to the sag sup sinus	40	58.5	1021

42



43



44

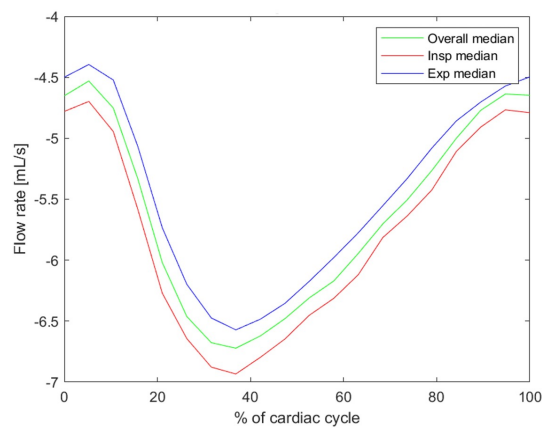
BBV

Signal	All	Insp	Exp	Δ Insp-Exsp	p-value of Δ
Mean AF	7.39±1.72	7.32±1.65	7.26±1.64	0.0607	0.068
Mean VF	-7.28±2.28	-7.35±2.45	-7.25±2.23	-0.0954	0.216
Mean CSFF	0.111±0.134	0.085±0.098	0.093±0.134	-0.0084	0.772
Syst AF	10.29±2.44	10.20±2.42	10.08±2.39	0.1244	0.059
Syst VF	-9.08±3.14	-9.21±3.35	-9.16±3.17	-0.0493	0.524
Syst CSFF	-1.81±0.60	-1.87±0.60	-1.80±0.62	-0.0733	0.062
Dia AF	5.11±1.37	5.02±1.26	5.02±1.26	0.0063	0.875
Dia VF	-5.90±2.05	-5.96±2.13	-5.88±2.08	-0.0830	0.310
Dia CSFF	1.44±0.53	1.38±0.42	1.41±0.42	-0.0267	0.416

Baselli...Lagana, Biosensors 2022

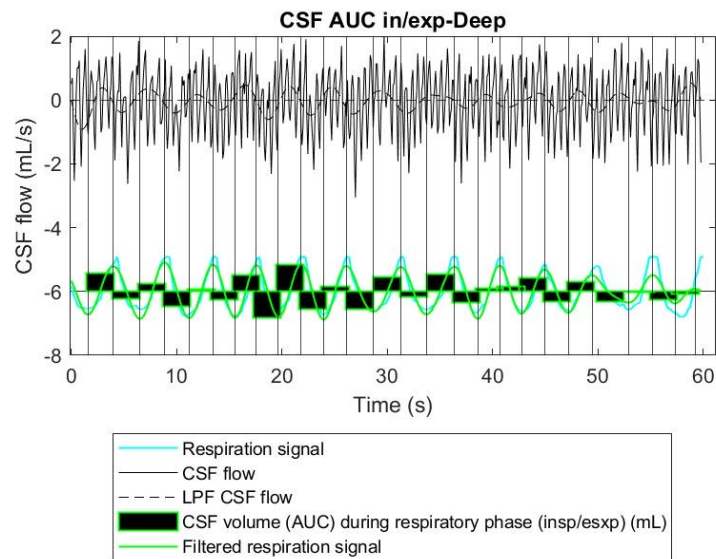
45

Inspiration and expiration



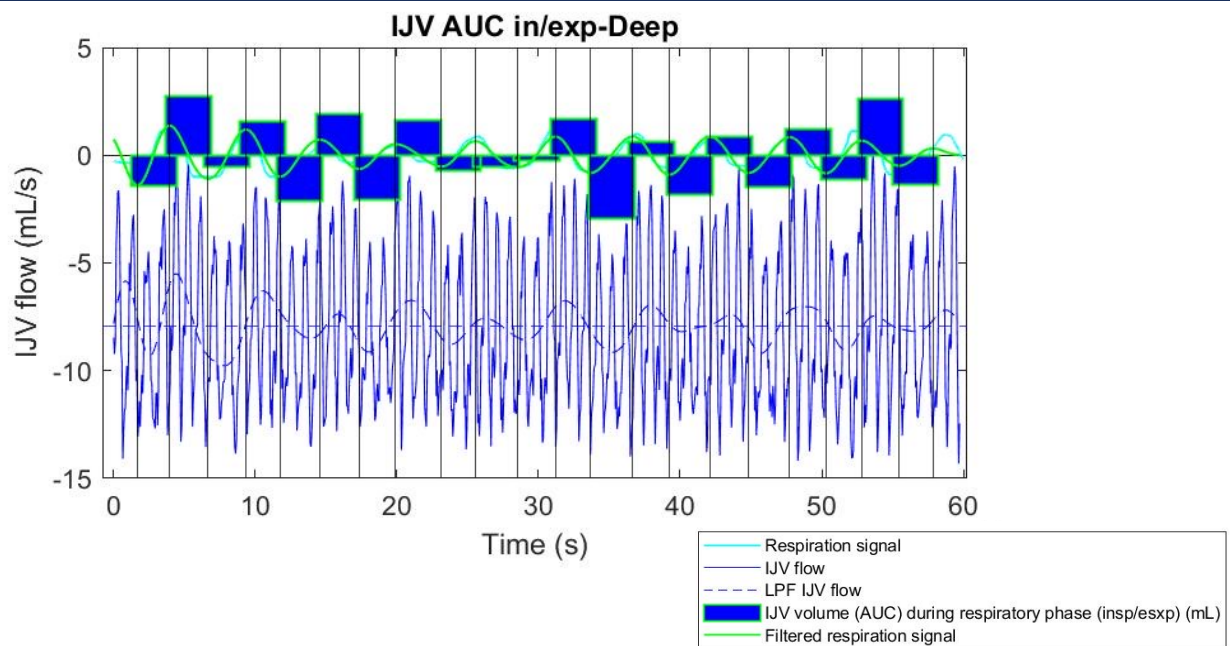
46

Flow volumes in inspiration and expiration



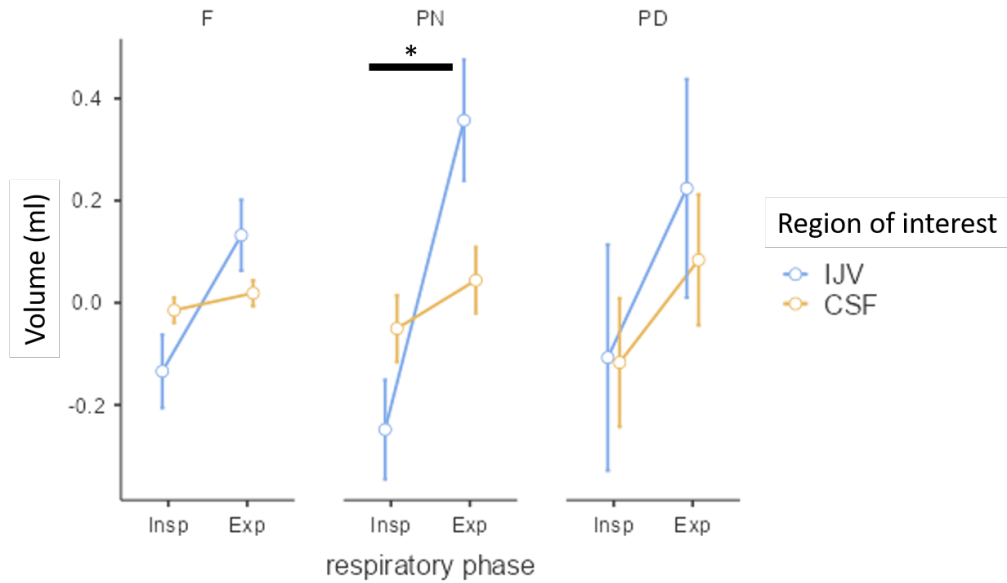
47

Flow volumes in inspiration and expiration



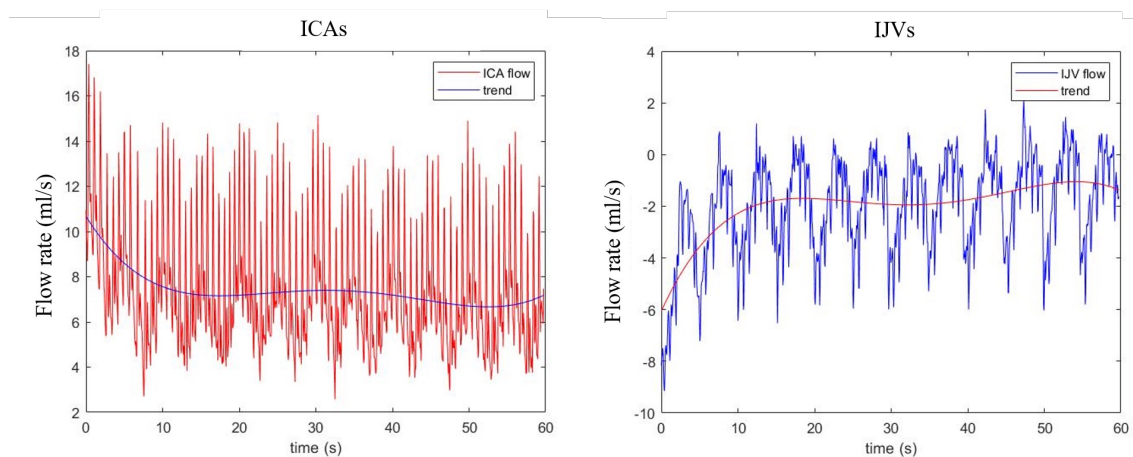
48

Flow volumes in inspiration and expiration



49

Flow rate: from free to deep breathing



50